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Regular recreational Cannabis users exhibit altered neural oscillatory dynamics during attention reorientation

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Abstract

Background. Cannabis is the most widely used illicit drug in the United States and is often associated with changes in attention function, which may ultimately impact numerous other cognitive faculties (e.g. memory, executive function). Importantly, despite the increasing rates of cannabis use and widespread legalization in the United States, the neural mechanisms underlying attentional dysfunction in chronic users are poorly understood.

Methods. We used magnetoencephalography (MEG) and a modified Posner cueing task in 21 regular cannabis users and 32 demographically matched non-user controls. MEG data were imaged in the time−frequency domain using a beamformer and peak voxel time series were extracted to quantify the oscillatory dynamics underlying use-related aberrations in attentional reorienting, as well as the impact on spontaneous neural activity immediately preceding stimulus onset.

Results. Behavioral performance on the task (e.g. reaction time) was similar between regular cannabis users and non-user controls. However, the neural data indicated robust theta-band synchronizations across a distributed network during attentional reorienting, with activity in the bilateral inferior frontal gyri being markedly stronger in users relative to controls ($p's$ < 0.036). Additionally, we observed significantly reduced spontaneous theta activity across this distributed network during the pre-stimulus baseline in cannabis users relative to controls $(p's < 0.020)$.

Conclusions. Despite similar performance on the task, we observed specific alterations in the neural dynamics serving attentional reorienting in regular cannabis users compared to controls. These data suggest that regular cannabis users may employ compensatory processing in the prefrontal cortices to efficiently reorient their attention relative to non-user controls.

Introduction

Following tobacco and alcohol, cannabis is the most widely used psychoactive substance in the United States (Azofeifa et al., [2016;](#page-7-0) Carliner, Brown, Sarvet, & Hasin, [2017\)](#page-7-0), with an estimated 24 million Americans aged 12 or older found to be current users of cannabis in 2016 (SAMHSA, [2017\)](#page-8-0). The main psychoactive component of cannabis is Δ^9 -tetrahydrocannabiol (THC), which acts, most notably, as an agonist of the endocannabinoid $CB₁$ receptor $(CB_1R;$ (Bloomfield et al., [2019\)](#page-7-0). CB_1R is a common G-protein-coupled receptor that is found in high concentrations in the neocortex (particularly frontal and limbic areas), hippocampus, amygdala, cerebellum, thalamus, and the basal ganglia (Bloomfield et al., [2019](#page-7-0)). Concomitant with widespread CB_1R activation are cognitive and behavioral changes that occur with acute (i.e. online, current use) and chronic cannabis use (i.e. persistent, repetitive use), including memory, executive functioning, and attentional deficits (Bloomfield et al., [2019;](#page-7-0) Broyd, van Hell, Beale, Yucel, & Solowij, [2016;](#page-7-0) Cohen & Weinstein, [2018;](#page-7-0) Ganzer, Bröning, Kraft, Sack, & Thomasius, [2016;](#page-7-0) Lovell, Akhurst, Padgett, Garry, & Matthews, [2019;](#page-8-0) Scott et al., [2018\)](#page-8-0). However, the neurobiological mechanisms underlying such cognitive dysfunction in the context of acute and chronic cannabis use remains poorly understood.

One behavioral hallmark of acute cannabis intoxication includes difficulty attending to pertinent stimuli in the environment, which may ultimately impact other cognitive domains including memory, executive, and motor functioning (Broyd et al., [2016\)](#page-7-0). While this relationship between cannabis use and the impairment of attentional domains (e.g. focused, divided, and sustained attention) is well established in acute users of cannabis (Broyd et al., [2016](#page-7-0); Cohen & Weinstein, [2018;](#page-7-0) Scott et al., [2018\)](#page-8-0), the effect of chronic, persistent cannabis use on attention function is far less understood (Broyd et al., [2016](#page-7-0); Cohen & Weinstein, [2018](#page-7-0); Ganzer et al., [2016\)](#page-7-0). In fact, the available data in this area is broadly conflicting (for an excellent review see Cohen & Weinstein, [2018\)](#page-7-0), although this may be related to methodological

considerations, including significant sample heterogeneity across studies. For example, inclusion criteria for chronic cannabis use varies widely from study to study, such as the amount of current use, the duration of use prior to study enrollment, and the duration of abstinence from cannabis use prior to study assessments (Ganzer et al., [2016](#page-7-0)). Recently, meta-analytical approaches (Lovell et al., [2019](#page-8-0); Schreiner & Dunn, [2012](#page-8-0); Scott et al., [2018](#page-8-0)) have helped clarify the cognitive effects of chronic cannabis use. Taken together, there seem to be reasonable agreement that there are attentional deficits associated with chronic cannabis use that become less severe and even insignificant when users abstain from the drug for an extended period. Another factor crucial to the impact of cannabis on cognitive function is the age at which individuals start using cannabis. Specifically, it has been demonstrated that participants who began using cannabis at earlier ages tend to have worse cognitive function (Bosker et al., [2013](#page-7-0); Hooper, Woolley, & De Bellis, [2014](#page-7-0)) and decreased cortical gray matter volumes (Wilson et al., [2000](#page-9-0)). Similar to the neuropsychological findings, neuroimaging studies have shown inconsistent results with regards to differences between cannabis users and nonusers. While some studies have found changes in brain morphology and activation patterns in cannabis users (Gilman et al., [2019](#page-7-0); Jager et al., [2007](#page-8-0); Lopez-Larson, Rogowska, & Yurgelun-Todd, [2015](#page-8-0); Schweinsburg et al., [2008;](#page-8-0) Wilson et al., [2000\)](#page-9-0), others have found no such differences between cannabis users and nonusers (Block et al., [2000;](#page-7-0) Jager, Kahn, Van Den Brink, Van Ree, & Ramsey, [2006;](#page-7-0) Tzilos et al., [2005\)](#page-8-0).

Productive daily life depends upon one's ability to orient and reorient their attention to behaviorally pertinent stimuli and information. These attentional processes are thought to be served by the interaction between two neural networks: the dorsal attentional network (DAN) and the ventral attentional network (VAN; Chica, Bartolomeo, & Lupiáñez, [2013;](#page-7-0) Corbetta & Shulman, [2002](#page-7-0); Corbetta, Patel, & Shulman, [2008](#page-7-0)). The DAN appears to be involved in top-down control processes based on current objectives and preexisting information, and includes activation of bilateral superior parietal lobules, intraparietal sulci, and frontal eye fields. In contrast, the VAN has been shown to be involved in bottom-up detection of goal-relevant stimuli (Corbetta et al., [2008](#page-7-0)), with key hubs in the right temporo-parietal junction and the ventral prefrontal cortices. Importantly, regions within both networks are activated upon the detection of behaviorally relevant targets and further amplified when attentional resources need to be reallocated to more behaviorally relevant stimuli (Corbetta et al., [2008](#page-7-0)). In addition to the neuroanatomical origins serving these attentional processes, recent studies have shown such activation comprises multispectral neural oscillatory responses within these networks during attention reallocation (Arif et al., [2020](#page-6-0)a, [b](#page-7-0); Proskovec, Heinrichs-Graham, Wiesman, McDermott, & Wilson, [2018;](#page-8-0) Spooner, Wiesman, Proskovec, Heinrichs-Graham, & Wilson, [2020](#page-8-0)).

While the neural processes serving attention and attentional reorientation have been extensively studied, the impact of regular cannabis use on these processes remains poorly understood. Thus, we examined the neural oscillatory dynamics underlying attentional reorienting in demographically matched users and nonusers using magnetoencephalography (MEG) and a modified Posner cueing task. The Posner task is a well-vetted attention paradigm that is commonly used to investigate the reorienting of attentional resources to novel target locations by either validity or invalidly cueing the participant to the location of the upcoming target stimulus, which induces a robust behavioral effect termed the validity effect (Arif et al., [2020](#page-6-0)a, [b](#page-7-0); Chica et al., [2013;](#page-7-0) Daitch et al., [2013;](#page-7-0) Macaluso & Patria, [2007;](#page-8-0) Posner, [1980;](#page-8-0) Proskovec et al., [2018](#page-8-0); Spooner et al., [2020;](#page-8-0) Thiel, Zilles, & Fink, [2004;](#page-8-0) Vossel, Thiel, & Fink, [2006;](#page-8-0) Vossel, Weidner, Driver, Friston, & Fink, [2012](#page-8-0); Wiesman & Wilson, [2019\)](#page-9-0). Importantly, the validity effect refers to a behavioral decrement (e.g. slowing reaction time) in response to invalidly cued targets, which are targets that appear in a different spatial location than the previous spatial cue. This effect is reflected in the brain through greater activation in key DAN and VAN nodes for invalidly cued trials compared to valid ones (Corbetta et al., [2008;](#page-7-0) Posner, [1980\)](#page-8-0). Based on previous literature, we hypothesized that the reorienting of attention would involve temporally sustained decreases in alpha and beta activity during target processing in DAN hubs (e.g. superior parietal lobules). In contrast, we predicted that there would be robust, transient increases in theta oscillatory activity in the VAN (e.g. inferior frontal cortices) during target processing (Arif et al., [2020](#page-6-0)a; Proskovec et al., [2018](#page-8-0); Spooner et al., [2020](#page-8-0); Wiesman, Groff, & Wilson, [2019](#page-8-0)). Considering the relatively low difficulty of the Posner task, we expected there to be little to no behavioral differences between the users and nonusers. Conversely, we expected there to be major differences in the oscillatory dynamics of users, indicative of compensatory neural mechanisms to maintain proper functionality compared to their nonuser counterparts, as has been shown in several major fMRI studies (Chang, [2006;](#page-7-0) Eldreth, Matochik, Cadet, & Bolla, [2004;](#page-7-0) Jager et al., [2006;](#page-7-0) Kanayama, Rogowska, Pope, Gruber, & Yurgelun-Todd, [2004](#page-8-0)). Finally, we also hypothesized that chronic cannabis users would exhibit alterations in spontaneous neural activity prior to stimulus onset, further indicative of disrupted neural processing in the brain regions serving attention function (Böcker et al., [2010](#page-7-0); Herning, Better, Tate, & Cadet, [2003](#page-7-0); Ilan, Smith, & Gevins, [2004](#page-7-0)).

Materials and methods

Participants

Fifty-three participants were enrolled in the study. Twenty-one active, regular cannabis users (7 females, mean age: 29.9, S.D.: 7.76) and 32 nonuser controls (13 females; mean age: 30.6, S.D.: 7.22). Exclusionary criteria included any medical illness affecting the central nervous system function, neurological or psychiatric disorder, history of head trauma, and standard exclusionary criteria for MEG (e.g. any type of ferromagnetic implanted material). After a complete description of the study, written informed consent was obtained from each participant.

Participants were identified as regular cannabis users based on the following criteria: (1) at least weekly cannabis use over the past 12 months, (2) current use of at least four times per week, and (3) not currently using any other illicit drugs (e.g. cocaine, heroin, etc.). Importantly, participants were asked to refrain from using any cannabis containing products on the day of their MEG appointment, to avoid any contamination of neural/ behavioral effects by acute substance use. Further, participants in the user group were screened for drug use on the day of examination to ensure that they were not using any drugs other than cannabis. In contrast, the nonuser group consisted of individuals with no current or past substance use, and were demographically matched to the user group based on age, sex, race, SES, and levels of depression (measured by the Beck Depression Scale). Of note, the groups differed on years of education and head motion during MEG, but inclusion of these variables in the final statistical models resulted in no changes to the results. Additionally, our

Fig. 1. Posner cueing task and behavioral performance. (A) A fixation cross was first presented for 1500 (±50) ms, followed by a cue (green bar) presented to the left or right of the fixation cross for 100 ms. After 200 ms, the target stimulus (box with opening) appeared in either the left or right hemifield for 2500 ms. Participants responded as to whether the opening was on the bottom or top of the target with their index and middle finger, respectively. Validly cued trials (cue location on the same side as the impending target) were presented for 50% of the trials, and a total of 200 trials (both valid and invalidly cued) were completed by each participant. (B) Behavioral performance of all subjects is shown on the y-axis (i.e. reaction time on the left, accuracy on the right) with condition (valid or invalid) on the x-axis. Reaction times were significantly slower during invalid trials compared to valid ones, while accuracy was unchanged as a function of task condition. *** $p <$ 0.001.

experimental groups were matched on current alcohol use as measured via the Alcohol Use disorders Identification Test – Consumption (AUDIT-C) scores (controls – M: 2.72, S.D.: 1.53; users – M: 4.05, S.D.: 2.85), to ensure that any cannabis-related effects in our data were not confounded by between-group differences in alcohol consumption.

Experimental paradigm

During the MEG recording, participants performed a modified Posner task (Posner, [1980\)](#page-8-0). As shown in Fig. 1 and described in prior works, each trial consisted of a fixation crosshair for 1500 ms $(\pm 50 \text{ ms})$, followed by a green bar (the cue) appearing on either the left or right of the crosshair for 100 ms, a 200 ms fixation cross, and then a target on either the left or right side for 2500 ms. Importantly, the target could be validly (i.e. same side as cue; 50% of trials) or invalidly cued. Each cue location (left or right) and target (valid/invalid) appeared an equal number of times and participants responded as to the location of the opening in the target stimulus (top/bottom) using their right hand on a nonmagnetic button pad. Each trial lasted 4300 ms (± 50 ms), with a total of 200 trials (100 valid, 100 invalid).

MEG data acquisition, preprocessing, and imaging

Neuromagnetic responses were sampled at 1 kHz using an Elekta/ MEGIN MEG system with 306 sensors. MEG data from each participant was individually corrected for head motion and subjected to noise reduction using the signal space separation method with temporal extension (Taulu & Simola, [2006\)](#page-8-0). The continuous magnetic time series was divided into epochs of 4000 ms duration, with the onset of the cue defined as 0 ms and the baseline defined as the 600 ms preceding the cue onset (−600 to 0 ms). Epochs containing artifacts were rejected based on a fixed threshold method. This process and the actual thresholds are described in the Supplemental Methods and, importantly, did not differ by group. Further, to ensure a balanced number of trials between groups and conditions, a mixed-model ANOVA was performed which showed no main effects of group, condition, nor interaction.

Artifact-free epochs were transformed into the time−frequency domain using complex demodulation (Kovach &

Gander, [2016](#page-8-0)). The specific time−frequency windows used for subsequent imaging were determined using a stringent statistical analysis involving nonparametric permutation testing of the sensor-level spectrograms across the entire array of gradiometers (see (Proskovec et al., [2018](#page-8-0); Spooner et al., [2020;](#page-8-0) Wiesman et al., [2018](#page-9-0)). Prior to image reconstruction, each participant's MEG data were coregistered to their individual high-resolution structural MRI using three fiducial points, four MEG coils, and the scalp surface, which was digitized using a Polhemus (Supplementary Methods). Using a spherical head model, cortical networks were then imaged at $4.0 \times 4.0 \times 4.0$ mm using the dynamic imaging of coherent sources beamformer (Gross et al., [2001\)](#page-7-0). The DICS approach utilizes the cross-spectral density matrices computed from the sensor-level complex demodulation to estimate the data dependencies. Following convention, these images were normalized per voxel using a separately averaged prestimulus noise period (i.e. baseline) of equal duration and bandwidth (Hillebrand, Singh, Holliday, Furlong, & Barnes, [2005](#page-7-0)). To assess the anatomical basis of the responses identified through the sensorlevel analysis, three-dimensional maps were computed across both conditions and then averaged across all participants. To examine the effects of cannabis use, virtual sensors (i.e. voxel time-series data) were extracted from each participant's data using peak voxels. For each coordinate of interest, the envelope of spectral power was computed for the frequency range used in the beamforming analysis. From this, we computed the relative (i.e. baseline corrected) and absolute (i.e. non-baseline corrected) response time series of each participant per task condition by averaging the absolute amplitude time series across the baseline period (i.e. −600 to 0 ms), and the relative time series across the time windows used for beamforming (i.e. theta: 350–700 ms; alpha/beta: 300–900 ms). Finally, mixedmodel ANOVAs were conducted to evaluate changes in task-related neural oscillations during target processing as a function of task validity, cannabis use, and their interaction, while two-sample t tests were used to assess differences in spontaneous baseline activity.

Results

Behavioral analysis

A mixed-model ANOVA of cue-validity, group, and their interaction on reaction time (RT) and task accuracy was conducted.

Fig. 2. Sensor-level analyses during attentional reallocation. Grand-averaged time −frequency spectrogram from a sensor near the left posterior parietal cortex, with time (ms) shown on the x-axis and frequency (Hz) denoted on the y-axis. A color scale bar shown above the spectrogram denotes the percent power change relative to the baseline period (-600 to 0 ms). The data per spectrogram have been averaged across all trials (both valid and invalid) and participants. Strong increases in theta (3– 6 Hz) were observed following cue (blue dashed line) and target (white dashed line) onset. Additionally, robust decreases in alpha (9–13 Hz) and beta (15–23 Hz) activity were observed following target presentation.

In regard to reaction time, we observed a significant main effect of cue validity $(F_{1,51} = 107.93, p < 0.0001)$, such that participants were significantly slower to respond to invalid $(M = 1030.2 \text{ ms}$, $S.D. = 145.7 \text{ ms}$ compared to valid trials $(M = 981.1 \text{ ms}$, $s.D. = 143.1 \text{ ms}$. Interestingly, there was no main effect of group ($F_{1,51}$ = 0.014, p = 0.907), nor a cue validity-by-group interaction on reaction time ($F_{1,51} = 1.663$, $p = 0.203$). In regard to task accuracy, we observed no main effect of cue validity $(F_{1,51} = 1.11,$ $p = 0.297$), group ($F_{1,51} = 3.94$, $p = 0.053$), nor validity-by-group interaction $(F_{1,51} = 1.11, p = 0.297)$.

Sensor-level analysis

Since the goal of the study was to investigate the oscillatory dynamics associated with attention allocation during target processing, we focused our analysis on the time periods following target presentation (i.e. after 300 ms). Statistical analyses of the time −frequency spectrograms during the target interval revealed significant clusters of theta (3–6 Hz), alpha (9–13 Hz), and beta (15–23 Hz) oscillatory activity across all participants and conditions (Fig. 2). The significant theta synchronizations began around 50 ms after target presentation and tapered off about 350 ms later (350–700 ms; $p < 0.001$, corrected). Strong desynchronizations in alpha and beta were much more temporally

extended with significant decreases beginning around the onset of the target interval and continuing for ∼600 ms (300–900 ms; $p < 0.001$, corrected).

Beamformer and virtual sensor analysis

Strong increases in theta activity were observed from 350 to 700 ms in the bilateral primary visual cortices, bilateral inferior frontal gyri (IFG), and right dorsolateral prefrontal cortex (dlPFC) ([Fig. 3,](#page-4-0) insets). In contrast, strong decreases in alpha activity were observed from 300 to 900 ms in the lateral occipital gyri (LOG) bilaterally, left primary motor cortex, and bilateral intraparietal sulci (IPS; see Supplemental Materials). In regard to beta, strong decreases were observed from 300 to 900 ms in the bilateral LOG, left primary motor cortex and right superior parietal lobule (SPL; [Figure 4](#page-5-0), insets). Importantly, alpha and beta decreases in the left primary motor cortex were not further evaluated, as previous work has tightly linked these responses to motor planning and execution processes (Heinrichs-Graham & Wilson, [2015](#page-7-0); Heinrichs-Graham, Arpin, & Wilson, [2016;](#page-7-0) Heinrichs-Graham, Kurz, Gehringer, & Wilson, [2017;](#page-7-0) Wilson, Fleischer, Archer, Hayasaka, & Sawaki, [2011](#page-9-0)), which are beyond the goals of the current study.

To quantify the spectrotemporal dynamics in these regions and evaluate differences in the processing of valid and invalid targets as a function of cannabis use, we used mixed-model ANOVAs with cue validity (valid/invalid), group (users/ non-users) and their interaction as factors of interest. Note that we did not collapse across hemisphere for frontal or parietal responses, as there is clear evidence of hemispheric specialization for attention function in these brain regions.

Theta activity increased during target processing in all four regions, with stronger activity elicited during the processing of invalid relative to valid trials (bilateral visual: $F_{1,50} = 15.20, p < 0.001;$ right DLPFC: $F_{1,50} = 24.47, p < 0.001;$ right IFG: $F_{1,48} = 52.24$, $p < 0.001$; left IFG: $F_{1,50} = 60.47$, p < 0.001). Activity in the left IFG also demonstrated a significant main effect of group, such that cannabis users exhibited stronger theta activity during target processing compared to controls $(F_{1.50} = 8.58, p = 0.005)$. Finally, we observed a significant cue validity by group interaction bilaterally in the IFG (left IFG: $F_{1,50} = 8.42$, $p = 0.006$; right IFG: $F_{1,48} = 4.68$, $p = 0.035$) and a trend towards significance in the bilateral visual cortices $(F_{1,50} = 4.03,$ $p = 0.0502$), such that greater theta activity during invalidly cued targets was accentuated in regular cannabis users compared to non-users [\(Fig. 3\)](#page-4-0). To ensure that the IFG responses were not related to saccadic eye movements during invalid trials, a supplemental sensor-level analysis was performed, and this showed that there were no detectable eye movements in the frontal sensors (online Supplementary Fig. S2).

In contrast to theta activity, alpha power decreased during target processing in the left and right IPS and LOG (online Supplementary Fig. S1). We observed stronger decreases in alpha power during validly cued compared to invalidly cued targets in all three brain regions (bilateral LOG: $F_{1,50} = 5.00$, $p = 0.030$; left IPS: $F_{1,50} = 4.35$, $p = 0.042$; right IPS: $F_{1,51} = 5.71$, $p = 0.021$), but there were no significant main effects of group nor interactions in any region ($ps > 0.447$).

Similarly, large decreases were also observed in the beta range throughout target processing in the bilateral LOG and right superior parietal lobule. Interestingly, stronger decreases in beta activity were observed during valid compared to invalid trials in the

Fig. 3. Theta activity during target processing. Theta beamformer images (inset top right of each panel) were computed across both conditions and then averaged across all participants. The images are shown in pseudo-t units following the neurological convention (right hemisphere on the right side). Increases in theta activity were observed in the following regions: (A) bilateral primary visual cortices, (B) right dorsolateral prefrontal cortex, (C) left inferior frontal gyrus, and (D) right inferior frontal gyrus. From the peak voxel exhibiting the strongest neural activity (yellow dot), time courses were extracted to evaluate changes in neural response as a function of group (controls: orange; users: blue) and task condition (valid: solid line; invalid: dashed line) during the target processing time window identified through the sensor level analysis (i.e. 350–700 ms; shaded area). Average reaction times across all participants for valid and invalid trials are denoted in red solid and dashed lines, respectively. Bar graphs represent the neural validity effect (i.e. invalid—valid) with error bars reflecting SEM. $*p$ < 0.05; #p = 0.0502. Insets showing occipital responses are in units of pseudo-t values scaled from 8.0 to 12.0 while the other insets are scaled from 5.0 to 6.0.

bilateral LOG ($F_{1,51} = 13.07$, $p = 0.001$), while this effect was not present in the right superior parietal lobule $(F_{1,50} = 0.971,$ $p = 0.329$; [Figure 4\)](#page-5-0). Additionally, while there were no main effects of group in either region ($ps > 0.603$), there was a significant cuevalidity by group interaction in the bilateral LOG, such that the neural validity effect (i.e. greater desynchronization during valid ν . invalid trials) was greater for regular cannabis users compared to non-users $(F_{1,51} = 9.28, p = 0.004;$ [Figure 4\)](#page-5-0).

Finally, we evaluated whether regular cannabis use affects spontaneous neural activity (i.e. basal activity) during the baseline, and found that spontaneous theta was significantly decreased in cannabis users relative to non-users in the primary visual cortices, bilateral IFG, and right DLPFC (ps < 0.020; [Figure 5](#page-6-0)). In contrast, baseline activity did not differ in any other regions exhibiting strong alpha/beta oscillations during target processing.

Discussion

We used a modified Posner cueing paradigm and MEG to investigate the oscillatory dynamics underlying attentional reorientation in cannabis users and nonusers, and observed robust multispectral modulation of dorsal and ventral attention networks (DAN and VAN, respectively) during attentional reallocation. Importantly, our study was the first to demonstrate cannabisrelated changes in task-induced neural oscillations in brain regions known to be critical for attention function. Below, these findings and their implications are discussed further.

Behaviorally, we observed a group-independent RT validity effect such that participants were slower to respond to invalid

trails relative to valid trials. This RT cost associated with attention reorientation has been well documented in the Posner cueing paradigm (Posner, [1980](#page-8-0), [2016](#page-8-0)). Interestingly, there were no group differences or group-by-cue validity interactions in RT or accuracy. These findings show that regular cannabis users in our study were able to perform at the same level as non-users on the Posner cueing task. Some studies (Bosker et al., [2013](#page-7-0); Dougherty et al., [2013](#page-7-0); Huijbregts, Griffith-Lendering, Vollebergh, & Swaab, [2014;](#page-7-0) Messinis, Kyprianidou, Malefaki, & Papathanasopoulos, [2006;](#page-8-0) Thames, Arbid, & Sayegh, [2014](#page-8-0)) have shown that chronic cannabis users perform worse than non-users while others (Hooper et al., [2014;](#page-7-0) Verdejo-García et al., [2013](#page-8-0)) have shown that both groups perform at the same level. Previously, this relationship between task performance and behavioral outcomes has been found to be task-dependent and influenced by the length of time since last using cannabis, such that, as the abstinence period increases, behavioral defects become less robust or even insignificant (Fried, Watkinson, & Gray, [2005;](#page-7-0) Hanson et al., [2010](#page-7-0); Lovell et al., [2019](#page-8-0); Roten, Baker, & Gray, [2015;](#page-8-0) Scott et al., [2018](#page-8-0)). Considering the short abstinence period (i.e. no use on the day of examination) used in the current study, the lack of behavioral differences between users and controls show that our task was relatively easy (i.e. 98.1% accuracy across group and condition), which was by design, and that any deficits in attention reorientation associated with regular cannabis use, at least as measured by the Posner cueing paradigm, were able to be internally overcome by users through neural compensatory mechanisms.

Recently, MEG analyses have specifically implicated IFG thetaband responses to be a key ventral network mediator involved in

Fig. 4. Beta activity during target processing. Beta beamformer images (inset) were computed across conditions and then averaged across all participants. The output images are shown in pseudo-t units following the neurological convention (right hemisphere on the right side). Decreases in beta activity were observed in the following regions: (A) lateral occipital gyri and (B) right superior parietal lobule. Time courses (i.e. line graphs) of beta activity from the peak voxel (i.e. yellow dot on beamformer images) in each region were averaged over the beamforming window (i.e. 300–900 ms; gray box) and the difference was calculated across conditions (i.e. invalid – valid) to determine the neural validity effect (bar graphs). Asterisks mark significant neural validity effects (p < 0.05), with error bars reflecting SEM. The inset showing occipital responses is in units of pseudo-t values scaled from 12.0 to 16.0 while the other inset is scaled from 13.0 to 21.0.

shifting the current attentional set to a new location (Proskovec et al., [2018;](#page-8-0) Spooner et al., [2020\)](#page-8-0). In the current study, significant cue-validity-by-group interactions were found in the bilateral IFG, such that, regular cannabis users exhibited significantly stronger theta responses during invalidly cued trials relative to validly cued ones compared to controls. Considering the importance of the prefrontal cortices in the reorientation of attention, it seems that regular cannabis users allocated greater neural resources to achieve the same level of attention reorientation as their non-user counterparts. Similarly, cue validity-by-group interactions approached significance ($p = 0.0502$) for theta responses in the bilateral primary visual cortices, and were significant for beta oscillations in the bilateral LOG. In both cases, the interactions were such that regular cannabis users had larger validity effects compared to non-users, although the directionality was reversed such that cannabis users had stronger theta oscillations in the IFG during invalid relative to valid trials and stronger beta LOG responses to valid relative to invalid trials compared to controls. The thetaband synchronization that was observed in the bilateral primary visual cortices is generally believed to reflect the initial encoding of visual stimuli (Fries, [2015](#page-7-0); Landau & Fries, [2012\)](#page-8-0), while the alpha- and beta-band desynchronization observed in the bilateral extrastriate regions have been associated with the detection of

specific stimulus properties (e.g. shape, color, and location) (Klimesch, [2012](#page-8-0); Neuper & Pfurtscheller, [2001](#page-8-0); Proskovec et al., [2018](#page-8-0)). Group differences in the strength of theta oscillations in the primary visual and IFG during invalidly ν . validly cued trials may reflect the dissemination of greater processing resources during invalid trials in regular users of cannabis. In regard to the stronger beta oscillations in the LOG during valid trials, this appeared to reflect both stronger and earlier responses during valid trials in cannabis users, with similar responses to invalid trials across groups.

In agreement with our findings, several studies in the domains of attention and working memory have found that, though neural differences existed between cannabis users and controls, there were no task-based behavioral differences between the groups (Chang, [2006;](#page-7-0) Eldreth et al., [2004;](#page-7-0) Jager et al., [2006](#page-7-0); Kanayama et al., [2004\)](#page-8-0). These results suggest that, at least in relatively easy tasks, cannabis users may be able to compensate to maintain the same level of task performance as their non-user peers, and our MEG findings provide at least some support for this contention. Such compensatory neural responses have been observed during task performance in the form of greater BOLD signal amplitude or duration in fMRI and/or the recruitment of neighboring cortical regions (Chang, [2006](#page-7-0); Eldreth et al., [2004;](#page-7-0) Jager et al., [2006](#page-7-0); Kanayama et al., [2004\)](#page-8-0).

Fig. 5. Spontaneous theta activity during the baseline period. Spontaneous theta activity averaged over the baseline period (−600 to 0 ms) is shown for each spatially defined peak in our beamformer analysis. Basal theta power was significantly reduced in all regions in chronic cannabis users compared to non-user controls. Asterisks mark significant baseline differences between groups ($p < 0.05$), with error bars reflecting SEM.

Another major finding of the current study was that regular cannabis use affected spontaneous cortical activity in attentionrelated brain regions. Previous work suggests that spontaneous neural activity prior to stimulus onset is modulated by healthy aging and disease-related processes (e.g. HIV-infection) (Casagrande et al., [2021;](#page-7-0) Heinrichs-Graham & Wilson, [2016;](#page-7-0) Lew et al., [2018;](#page-8-0) Rossiter, Davis, Clark, Boudrias, & Ward, [2014;](#page-8-0) Spooner et al., [2018](#page-8-0); Spooner, Wiesman, Proskovec, Heinrichs-Graham, & Wilson, [2019](#page-8-0); Wiesman et al., [2018](#page-9-0)). In the current study, we found significant decreases in pre-stimulus theta power in the bilateral primary visual cortices, bilateral IFG, and right dlPFC in regular cannabis users relative to controls, while pre-stimulus alpha and beta activity was unaffected by cannabis use. In regard to mechanism, in vivo and in vitro animal studies have demonstrated that CB_1Rs on GABAergic interneurons in the cerebral cortex and hippocampus, which are regulated by the endocannabinoid system, mediate theta- and gamma-band (30–80 Hz) oscillations (Hajos et al., [2000](#page-7-0); Hajos, Hoffmann, & Kocsis, [2008](#page-7-0); Katona et al., [1999](#page-8-0); Morgan, Stanford, & Woodhall, [2008;](#page-8-0) Robbe et al., [2006;](#page-8-0) Skosnik et al., [2012](#page-8-0)). The disruption of GABAergic interneurons by exogenous CB_1R agonists (e.g. THC) is thought to mediate decreased baseline theta and gamma power in cannabis users (Skosnik et al., [2012](#page-8-0); Skosnik, Cortes-Briones, & Hajós, [2016](#page-8-0)). Specifically, such decreased pre-stimulus theta power has been demonstrated in both acute cannabis use (Böcker et al., [2010;](#page-7-0) Ilan et al., [2004](#page-7-0)) and in abstinent regular users (Herning et al., [2003](#page-7-0)). As such, it is not surprising that theta band spontaneous activity was found to be disrupted in our study of regular cannabis users. Furthermore, the chronic administration of CB_1R agonists (e.g. THC) has been shown to cause a dramatic down-regulation and desensitization of CB_1 receptors throughout the brain (Bonnet & Preuss, [2017;](#page-7-0) Sim-Selley, [2003](#page-8-0)). Studies suggest that it takes about one month of abstinence for CB_1R binding to normalize, and this timeframe roughly corresponds to the duration of cannabis withdrawal syndrome (CWS; Bonnet & Preuss, [2017](#page-7-0)). Interestingly, an EEG study by Herning et al. ([2003\)](#page-7-0) found that decreased resting state theta power in regular cannabis users persisted for 28 days of monitored abstinence. Taken together, we believe that the decreased spontaneous theta power observed in regular cannabis users is likely related to disruption of GABAergic interneurons by exogenous CB_1R agonists and CB_1R habituation (i.e. downregulation and desensitization).

Before concluding, it is important to note the limitations of this study. First, each cannabis user in our study consumed their own cannabis day-to-day, and thus there were likely individual differences in the potency (i.e. concentration of cannabinoids), route of administration (e.g. smoke, dab, edible consumption, etc.), and composition (i.e. relative amounts of THC and CBD) of the consumed cannabis. These differences may be important because CBD may offset some of the effects of THC (Bloomfield et al., [2019\)](#page-7-0) and minimize the harm (Weinstein, Livny, & Weizman, [2016](#page-8-0)). Second, there were differences in the duration of cannabis use in our sample and the impact of such duration differences is unknown. Future studies should directly focus on the impact of duration and potency. Third, the current study utilized relatively small sample sizes and future studies would benefit from including more participants. Additionally, nicotine and caffeine consumption were not directly controlled for in the current study. Finally, all of the cannabis users in our study were recreational users and thus our findings may not extend to medicinal users or those who use for both purposes.

To close, the current study was first to investigate alterations in the neural oscillatory activity underlying attentional reorienting in regular, recreational cannabis users. Briefly, we found that cannabis users had significantly altered oscillatory dynamics in key regions of the DAN and VAN during attentional reallocation relative to controls, as well as altered spontaneous theta in some of the same brain regions. Some of these oscillatory differences may serve a compensatory role and help users to maintain adequate performance. Future studies should further investigate the nature of such neural oscillatory differences and their role in maintaining task performance. Considering the regulatory shifts in the United States and other countries relating to the legality of cannabis use, it is becoming increasingly important that the effects of regular cannabis use are more thoroughly understood, and consequently further research on the cognitive and physiological effects are seriously needed.

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The authors assert that all procedures contributing to this work comply with the ethical standards of the relevant national and institutional committees on human experimentation and with the Helsinki Declaration of 1975, as revised in 2008.

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